Tendon neuroplastic training: changing the way we think about tendon rehabilitation: a narrative review

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ABSTRACT
Tendinopathy can be resistant to treatment and often recurs, implying that current treatment approaches are suboptimal. Rehabilitation programmes that have been successful in terms of pain reduction and return to sport outcomes usually include strength training. Muscle activation can induce analgesia, improving self-efficacy associated with reducing one's own pain. Furthermore, strength training is beneficial for tendon matrix structure, muscle properties and limb biomechanics. However, current tendon rehabilitation may not adequately address the corticospinal control of the muscle, which may result in altered control of muscle recruitment and the consequent tendon load, and this may contribute to recalcitrance or symptom recurrence. Outcomes of interest include the effect of strength training on tendon pain, corticospinal excitability and short interval cortical inhibition. The aims of this concept paper are to: (1) review what is known about changes to the primary motor cortex and motor control in tendinopathy, (2) identify the parameters shown to induce neuroplasticity in strength training and (3) align these principles with tendon rehabilitation loading protocols to introduce a combination approach termed as tendon neuroplastic training. Strength training is a powerful modulator of the central nervous system. In particular, corticospinal inputs are essential for motor unit recruitment and activation; however, specific strength training parameters are important for neuroplasticity. Strength training that is externally paced and akin to a skilled movement task has been shown to not only reduce tendon pain, but modulate excitatory and inhibitory control of the muscle and therefore, potentially tendon load. An improved understanding of the methods that maximise the opportunity for neuroplasticity may be an important progression in how we prescribe exercise-based rehabilitation in tendinopathy for pain modulation and potentially restoration of the corticospinal control of the muscle-tendon complex.

INTRODUCTION
The clinical outcomes of treatment of tendinopathy vary—there is currently no single effective treatment. Unimodal interventions aimed solely at peripheral tissue, in this case the tendon, are unlikely to address complex corticospinal and neuromuscular adaptations associated with persistent pain. In this paper, the term *corticospinal control of the muscle* will refer to motor unit activation as a result of excitatory and inhibitory corticospinal inputs onto the spinal motor neuron pool, which will ultimately affect tendon loading and motor performance. Therefore, it is logical to explore the corticospinal pathway in people with tendinopathy.

Given the high incidence of bilateral tendinopathy[1] and bilateral pathology with predominantly unilateral load in animal[2] and human studies,[3] it is also important to consider the corticospinal control of the non-painful side in tendinopathy. A frequent and frustrating phenomenon is the clinical presentation of the previously unaffected side following rehabilitation. These observations pose several clinical questions: what are the differences in motor control between those people with tendinopathy and those without (that may predispose people to tendinopathy or may be adaptations)? Are there side-to-side differences associated with unilateral tendinopathy? How well does our current rehabilitation therapy address these issues of motor control?

MOTOR CONTROL IN PEOPLE WITH AND WITHOUT TENDINOPATHY
In tendon research, muscle strength, usually represented by maximal voluntary contraction (MVC), is far more often evaluated than is motor control. Interestingly, there is no consistent pattern of strength or performance change (either increase or decrease) in those tendons that have been studied (or the contralateral limb) and this may conflict with the clinical perception that pain is likely to result in strength loss due to disuse or willingness to protect the injured part consciously or subconsciously. For example, people with rotator cuff (RC) tendinopathy have been shown to be 15% stronger in measures of abduction on their asymptomatic side than controls (and comparable in strength to controls on their symptomatic side),[4] and this has also been seen in lateral epicondylalgia.[5] Athletes with patellar tendinopathy (PT, also termed jumper's knee) have been shown to be better jumpers than athletes without jumper's knee[6 7]; however, several studies report less strength on the symptomatic side than in controls (see Heales et al[8] for review). It is also reported that full strength is not recovered after surgery for Achilles tendinopathy.[9] There is no convincing association between strength deficit and presence of tendinopathy, as demonstrated by several studies.[8]

People with PT displayed greater cortical inhibition in their quadriceps responses[10] than healthy individuals.[11] Increased cortical inhibition has been shown to be associated with phasic (occurring in phases/intermittent) nociceptive stimuli,[12] which

describes tendon pain is consistently linked with loading and therefore, often phasic rather than tonic (sustained) for many tendons. While there was increased cortical inhibition altering motor drive in PT, there was also greater corticospinal excitability (CSE) than in controls inferring differences in the balance of excitability and inhibition of motor control as compared with healthy controls (Rio *et al*, in press). It may be that strength changes still represent a decrease from that individual's potential performance.

A recent systematic review by Heales *et al*[8] on the sensory and motor deficits of the non-injured side of patients with unilateral tendon pain included one study on the patellar tendon and one study on the Achilles tendon; however, there were 18 studies on the upper limb tendons. There is clearly a paucity of literature investigating lower limb sensory and motor changes in tendinopathy. The included lower limb studies measured arch height in PT[13] and Achilles tendon structure with imaging.[14] It is not clear how arch height and imaging changes may relate to sensory or motor changes; thus, the sensory or motor changes in lower limb tendinopathy require further investigation. This bias towards upper limb studies was paralleled by a recent systematic review on complex regional pain syndrome, which only identified suitable data from upper extremity studies.[15] It is possible that differences in functional reorganisation in the primary somatosensory (and/or primary motor cortex (M1)) cortices following upper limb versus lower limb injury may exist that limit the extrapolation of upper limb findings to the lower limb. Given that the predominant role of the upper limb musculature relates to position and control of the hand in space, and that the hand is well represented on the somatosensory cortex and M1, injury to upper limb regions may have manifestations associated with chronicity that are different from those in the lower limb. There appears to be a bias towards investigations of upper limb conditions.

The cross-sectional design of all studies that have investigated motor control in tendinopathy makes it difficult to infer causality and the potential impact of handedness or hand-use profiles (especially in upper limb studies).[16–18] That is, there is a more complex relationship at play: talented jumpers are more likely to play in positions that require more jumping (eg, in volleyball, as an outside hitter rather than a setter);[19] thus, such participants may be more vulnerable to tendon pain in their dominant limb, which is likely to have been stronger than their other one to begin with. These factors will also affect measures of strength and the stimulus response characteristics of primary motor cortex (M1) cells. Furthermore, maximal strength performance data are vulnerable to cognitive and motivational factors.[20 21] More importantly, maximum strength measures may not reflect the complex interaction between excitatory and inhibitory influences on the motor command that occur during tasks.

Indices of maximum strength may not provide enough detail about muscle-tendon loading at submaximal levels, nor have the ability to grade muscle recruitment[22] or appropriately timed patterns of activation according to the required task, especially in a painful state (eg, see Hodges and Richardson,[23] and Wadsworth and Bullock-Saxton[24]). Each of these scenarios have significant implications for function and load attenuation.[25] Transcranial magnetic stimulation (TMS) studies have shown that athletes with PT have greater M1 excitability than pain-free jumping athletes, as reflected in larger evoked muscle responses in the quadriceps (rectus femoris; Rio *et al*,[10] in press). As stated, athletes with PT also have greater cortical inhibition than healthy controls have.[11 26 27] That the investigation of these issues involves identical loading and contextual environment

across patient and control groups clearly points to an imbalance between the excitatory and inhibitory influences over muscle activation around the painful tendon. There may be several mechanisms that underpin these problems, not least changes in the response profile of clusters of neurons in M1, but the exact mechanisms remain to be untangled. Nonetheless, the functional result seems consistent with a protective adaptation that reduces the mechanical demands placed on the tendon, that is, an apparently protective adaptation.

Jumping and landing mechanics will be influenced by motor control changes that include both peripheral and central contributions to lower limb activation. People with patellar tendon abnormality (pathologically observable on ultrasound) have demonstrated landing patterns different from those of controls and importantly, have less variability in movement than healthy controls.[28] Movement variability is thought to minimise load accumulation in a specific region and reduced variability may be observed in, for example, reduced coefficient of variation in knee joint angles during a landing task.[29] The invariable motor pattern implies that corticospinal control is altered in some way and may be due to protective strategies underpinned by evaluative processes relating to the consequence or meaning of the motor task.[30] In the case of patellar tendon abnormality, invariable motor patterns may reflect a strategy to avoid pain during jumping (consequence) as well as the competing desire for optimal performance (meaning). In fact, better jumping ability has been shown to be a risk factor for developing PT[31] and indeed, people with PT are better jumpers or at least as good as those without—termed the 'jumper's knee paradox'.[6 7 32]

Less variability has been observed in asymptomatic controls who demonstrate a protective postural strategy when they expect their back to hurt,[33] and people with recurrent back pain demonstrate a protective strategy even when they are pain free.[34] Moreover, a reduction in normal variability of postural adjustments has been observed during experimentally induced pain, and failure to reinstate normal variability has been proposed as a possible risk for recurrence.[30] Such findings raise the possibility that an invariable motor pattern observed in PT may reflect a system less adaptable to environmental perturbations—an undesirable state.[35] Indeed, movement variability has been proposed as an important feature in actually preventing injury.[36]

Though the predicted goal of adopting a different motor strategy is protection, non-resolution of the strategy may in fact increase the likelihood of symptom recurrence.[30] Given the high recurrence rate of tendinopathy, it is pertinent to consider that there may be non-resolution of motor strategies even in currently asymptomatic people with a history of tendon pain, or tendon pathology, that predisposes them to symptoms or symptom recurrence. This outcome may also reflect the competing desires for optimal performance and tissue protection. This adds complexity to the design and implementation of rehabilitation, as the strategy (movement pattern) adopted will reflect competing desires of performance and protection, particularly if there has been no change to inputs (of which nociception is only one). To provide a clinical example, the presence of a positive 'culture' of PT in jumping sports, such as volleyball where playing with tendon pain is common (and may reinforce a concept that pain during activity does not equate to tissue damage), will probably serve to maintain the motor control strategy. These contextual factors are likely to further influence the experience of pain,[37] and will vary depending on the environment and one's own experiences.

Cross-sectional studies do not allow elucidation of whether tendon pathology or the presence of tendon pain precedes

changes in motor control. That pain will often be accompanied by altered motor output would be predicted on the basis that both pain and motor output can be effective at protecting us from bodily threat. A common finding in studies of motor control during pain is altered corticospinal drive to the motor neuron/muscle. However, this phenomenon of greater CSE has also been observed during testing that was non-painful, in people with PT as compared with activity-matched controls and people with other anterior knee pain (Rio et al, accepted). Furthermore, there were no differences between groups for activity, muscle strength (measured by maximal voluntary isometric contraction torque of the quadriceps), muscle activation (represented by surface electromyography) or measures of motor neuron activation (maximal femoral nerve stimulation); so it seems plausible that the increase in CSE was associated with the PT regardless of the fact that there was no pain during testing. It is possible that their net motor drive to the quadriceps muscle group is unaltered (or even that they may not be as good as they could be); however, controlled activation and the motor strategy may be affected. This also implies the motor task still has potential 'consequence' and 'meaning' in the absence of nociception, which fits with the invariable and abnormal landing strategy observed in people with tendon pathology.

Current tendon rehabilitation may fail to adequately address the multitude of contributing factors to altered motor control, which would include not only muscle strength and tendon capacity, but corticospinal control encompassing excitability and inhibition as well as belief systems about pain and contextual factors.

Motor control changes may be bilateral

The lack of consistent abnormalities in muscle strength on the patient's affected leg may simply reflect similar abnormalities being present on the contralateral limb. Heales et al[8] reported that the contralateral asymptomatic side was weaker than controls in upper limb tendinopathy, though abduction in those with RC tendinopathy was an exception and no data were reported for the lower limb. Interestingly, data from low back pain studies are also variable with some reporting both hypoactivity and others reporting hyperactivity, depending on the muscles and tasks investigated (see Hodges and Moseley[38] for review). Strength deficits persist following surgery and rehabilitation in unilateral Achilles tendinopathy; however, the side-to-side strength difference was relatively low (7.2–8.8%) and may actually reflect a bilateral motor control deficit.[9] However, while the direction of change (increases or decreases in muscle performance) is not consistent, it does appear that a change in motor control may occur bilaterally.

Regardless of whether motor control changes are a cause of pain or epiphenomena, changes to motor control may not just be bilateral but system wide. There is an increasing body of evidence that multiple sites are frequently affected due to complex intrinsic and extrinsic factors, and contralateral pathology and/or the development of symptoms is common. That is, once tendon pain (or pathology) is established at one site, there appears to be the potential for increased risk of tendinopathy elsewhere. Notwithstanding systemic risk factors that predispose tendinopathy, such as diabetes, elevated cholesterol and genetic factors (eg, the COL5A1 genotype in isolation[39] or in combination),[40] there may be other considerations, including an increase in global sympathetic drive.[41] While it is likely that loading is similar for both legs and bilaterality of pathology (and/or pain) may be, therefore, somewhat expected, data from the upper limb with markedly different use profiles (such as

baseball pitchers)[3] and unilaterally loaded animal models that demonstrate bilateral pathology[2] implicate systemic or nervous system involvement in tendinopathy. The interhemispheric connections and potential for modulation at the spinal cord level are both potential avenues for bilateral changes outside of bilateral loading that have not been as yet investigated.

It is possible that the other side may display differences in response to unilateral nociception (or insult) similar to what is observed in injury such as stroke. The adaptive response seen following stroke includes increased inhibition on the affected side and increased CSE to the unaffected limb.[42] Furthermore, there is actually increased interhemispheric inhibition from the non-affected hemisphere to the lesioned hemisphere that further increases the inhibition on the affected side during activation of the unaffected limb.[42] This perhaps has a biological advantage to improve efficiency of the unaffected side; however, this remains a challenge in rehabilitation (as the affected side has significant inhibition and is further increased during activation of the unaffected limb).

To investigate the unaffected side in people with PT, 13 jumping athletes (6 control participants, 7 with unilateral PT) were recruited (Rio, unpublished data available as an online supplementary material). Participants were tested bilaterally with TMS including their active motor threshold and a stimulus response curve as well as short interval cortical inhibition (SICI) using rectus femoris as the target muscle. When compared with healthy, activity-matched controls, preliminary data in athletes with PT demonstrate hyperexcitability on their affected side, supporting previous research (Rio et al, unpublished, available as an online supplementary material) and also displayed markedly increased cortical inhibition (n=4 affected side SICI ratio 17.12%, n=6 controls 58.78%). This motor control strategy may be likened to a novice driver controlling the speed of their car with one foot on the brake and one on the accelerator. Interestingly, the contralateral pathway controlling the unaffected side appears less excitable than both the affected side (similar to that observed in stroke) and controls, and also displays increased cortical inhibition (n=4 unaffected side 19.13%; where lower SICI percentage ratio represents greater cortical inhibition). These preliminary findings appear to replicate the findings of unilateral stroke that affects the M1, in particular the plausibility of greater interhemispheric inhibition and involvement of bilateral changes. However, the sample size is small and warrants further investigation with greater numbers. It does, nevertheless, highlight the danger of using the unaffected side as a control in studies of motor control, excitability or inhibition in people with tendinopathy. This also requires further evaluation as the clinical implications are considerable—strength training in the affected limb may continue to drive inhibition to the unaffected limb unless we can improve our understanding of techniques that modulate excess inhibition.

Given the propensity for lower limb activities to be bilateral and symmetrical for efficiency (ambulation, jumping, etc), the changes in the unaffected side may be an attempt to achieve motor control homoeostasis in a system trying to protect a region. That is, there are combined and perhaps competing demands of protecting a vulnerable or potentially vulnerable tendon while still producing torques sufficient for optimal performance. This may be argued for many tendinopathies not just in athletes, but in people involved in manual labour or any outcome-dependent task.

The contralateral motor control changes may also contribute to or explain the high injury rate of the contralateral tendon following rehabilitation. That is, loading patterns in the

contralateral limb are likely to be different as corticospinal drive of the unaffected side is altered. This provides support for a rehabilitative strategy that targets the corticospinal control of both sides; however, these strategies may need to be carefully considered. Strategies that modulate inhibition on the affected side as well as pain, such as isometric muscle contractions in PT,[10] should be evaluated for their potential effect on interhemispheric inhibition and inhibition of the ipsilateral M1. Rehabilitation that is capable of modulating pain *and* inhibition of both M1 may yield important advances in tendon management.

THE KEY QUESTION IS WHAT HAPPENS FIRST?

There are two theories about the relationship between pain and changes in muscle control (see Hodges and Moseley[38] for review), and neither is supported unequivocally by the literature. They propose that either changes in muscle activity cause pain (sometimes termed pain-spasm-pain model or vicious cycle of pain in the pain literature) or that changes in muscle activity serve to protect the area by limiting movement (the pain adaptation model).[43]

Experimental pain studies that demonstrate transient changes to motor control after a transient nociceptive stimulus,[44–46] as well as studies on a number of chronic conditions provide support for the pain adaptation model.[43] The definitive study that studies motor control before the onset of pain remains elusive.

Hyperexcitability of the quadriceps in athletes with PT has been correlated with length of time of symptoms (Rio, unpublished data available as an online supplementary material) and changes in infraspinatus excitability in people with RC tendinopathy were correlated with chronicity.[47] This does not exclude the possibility that aberrant motor control precedes the first onset of tendinopathy but provides a strong rationale that changes in motor control occur in response to nociceptive barrage. The potential for unilateral nociceptive input to drive motor control changes bilaterally (or possibly even system wide) underlines the importance of improving our understanding of nociception-motor interactions,[48] particularly in a condition of chronic nociception where the nociceptive driver is unknown.

The pain adaptation model proposes that agonist activity is reduced and the antagonist activity is increased with pain.[43] This may be the case in PT as there were no differences in MVC between athletes with PT and controls (Rio *et al*, accepted). However, in a separate study, following isometric exercise that reduced their pain, the MVC of the quadriceps of athletes with PT increased by 18.7%, implying their agonist activity (the quadriceps) was in fact inhibited (reduced) prior to isometric exercise.[10] The hamstrings that serve as the antagonists have not been measured. Most testing is completed in the laboratory with a single joint movement for simplicity, for example, leg extension; however, agonists and antagonists would change during a more complex movement such as a counter movement jump.

The threat to tissue (as far as the brain is concerned) may remain even after pain reduction and return to sport, as tendon may not have 'healed' (many consider tendinopathy to be failed healing; see Cook and Purdam[49] for review). In this context, there may be ongoing monitoring and persistent changes to corticospinal control of muscle (to protect the tendon) as the M1 and its projections may consider it to be vulnerable. Alternatively, the motor control changes that occur in tendinopathy may not spontaneously resolve or normalise following recovery, thus indicating rehabilitation may not address motor

activation and leaving people vulnerable to recurrence of symptoms.

People can and do recover in terms of pain and function despite tendon pathology remaining unchanged on clinical imaging.[50] One plausible explanation for this, at a tissue level, is that the tendon may structurally compensate in the area around the pathological lesion. That is, the volume of structurally intact tissue increases as an adaptive response.[51] This tendon may be thicker but potentially amenable to improvements in mechanical strength[51] through graded rehabilitation that would also alter muscle properties. The reverse is also observed, however, where patients can have symptoms without demonstrable structural pathology and reminds us that there is a disconnect between structure and pain (see Rio *et al*[52]). Non-painful motor activation would also improve self-efficacy; so there are a number of potential mechanisms linking rehabilitation (in particular strength training) to improvements in symptoms. However, given the clinical observation that 'once a tendon, always a tendon' reflects the strong tendency for symptom recurrence, there is clearly room for improvement in our strategic approach. Given the differences in motor control observed across tendinopathies, how well does current rehabilitation address motor control?

RESISTANCE TRAINING AND MOTOR CONTROL

Muscle activation involves activation of broad cortical and subcortical regions.[53 54] Self-paced resistance training describes a process without external timing cues (such as visual or auditory). In the clinical setting, an example of self-paced resistance/strength training may be where a patient is advised to complete three sets of 10 contractions lifting a certain weight—it is without advice about the timing of the contraction (eccentric and concentric phase) nor are there timing cues, such as a metronome sound, to provide structure to the timing of the contraction. Studies that have used external pacing, for example, with a metronome where the individual would contract concentrically and eccentrically to the sound of the metronome and complete these phases exactly as prescribed or follow a visual cue to match the pace of the contraction phases, have demonstrated increases in excitability in both skill (visuomotor tracking)[55] or short-term resistance training.[56–58] Leung *et al*[58] investigated the effects on excitability and inhibition of a single bout of visuomotor tracking compared with self-paced resistance training and metronome-based resistance training. They found that both skilled training and metronome-paced resistance training, but not self-paced resistance training, increased excitability and released inhibition in both the trained limb and in the untrained limb. This has implications for tendinopathy rehabilitation as both CSE and inhibition have been shown to be different compared with controls.

CURRENT TENDON REHABILITATION AND PROPOSED CONCEPT

Current rehabilitation aims to restore tendon and muscle properties using exercise with a variety of paradigms. There is evidence for the efficacy of eccentric-only contractions[59–64] and heavy slow resistance (involving both a concentric and eccentric component)[65] in improving pain and function in Achilles and PT. Protocols that include strength training (load) appear to provide the greatest stimulus for the tendon and muscle.

However, deficits in muscle performance have been shown to persist following surgical intervention plus rehabilitation or rehabilitation alone for tendinopathy, despite positive clinical outcomes.[9 66] Current prescription of tendinopathy

rehabilitation is best described as self-paced where patients are provided exercises with guidance of repetitions, sets and load (all of these are variable and no gold standard exists) but, importantly, without external pacing (either visual or auditory). Given the high recurrence rate of tendinopathy and persistent motor changes following rehabilitation,[66] it is possible that current rehabilitation fails to restore corticospinal control of the muscle-tendon complex(s).

Rehabilitation protocols are historically directed at local tissue adaptation (muscle hypertrophy and tendon) and there has been little, if any, focus on modulating corticospinal control. It is possible that these approaches, therefore, only address some of the neuromuscular and muscle-tendon changes in tendinopathy. Furthermore, passive unimodel treatments, such as injections, are unlikely to address local or central deficits such as tendon capacity, muscle strength across the kinetic chain and these issues of excitability and inhibition (figure 1A–D).

Externally paced resistance training, such as with the use of a metronome, is capable of inducing ipsilateral and contralateral changes to the excitability and inhibition in healthy participants.[11 57 67–69] To investigate this concept in a PT model, a protocol was developed that used externally paced strength training, termed tendon neuroplastic training (TNT) (protocol available in Rio *et al*, submitted and online supplementary material). Two strategies were trialled, either isometric or isotonic quadriceps muscle contractions, using TNT (the combination of heavy strength training and externally pacing) due to a lack of efficacious in-season loading options and both active treatments. This had a clinical basis to answer the questions: which programme may reduce pain immediately in-season and, was there any difference between them over a 4-week trial? As both groups were externally paced with the training, it was hypothesised they would both improve in excitability and inhibitory control. However, one protocol may be better for analgesia and this may also affect control, particularly cortical inhibition.

A subgroup of 9 athletes completed the corticospinal testing before and after the 4-week TNT intervention (that recruited 29 athletes) and 1 of the athletes completed weekly testing (figure 2). An online supplementary material is available with the method and full data set.

Isometric exercise provided greater immediate analgesia (Rio *et al*, submitted) and both protocols reduced pain significantly over the 4-week trial (van Ark *et al*, submitted). There were no differences between groups after 4 weeks. A case study demonstrates that there are changes in excitability over the course of 4 weeks and week 4 most closely represents normal CSE in jumping athletes without PT.

Testing showed that TNT, using either isometric or isotonic muscle contractions, changed inhibition (p=0.008; figure 3).
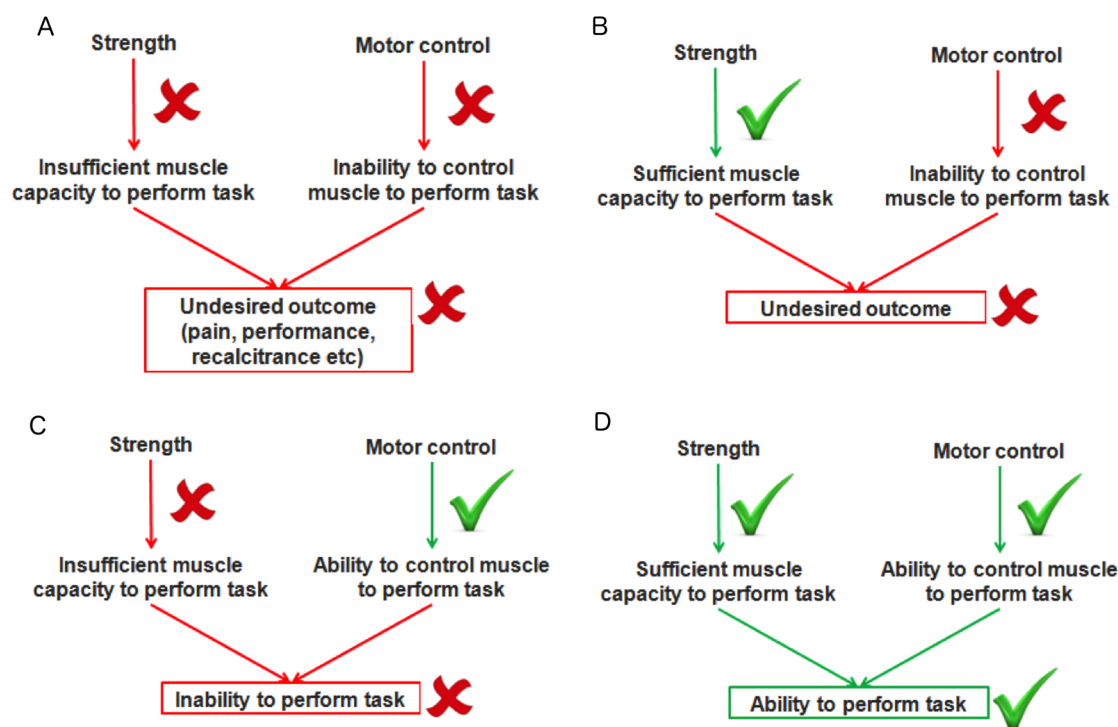

Figure 1 Summary of different approaches of tendon rehabilitation, and effects on strength and motor control. (A) Passive intervention fails to address strength and capacity of the tendon or muscle as load is required to stimulate these tissues; this leads to an inability to perform the task and an undesired outcome on the left. An example may be an injection into the tendon aimed at restoring tendon structure. Simultaneously, motor control has not been addressed; thus, the drive to the muscle may be unchanged and the outcome remains undesirable. (B) This likely describes most current clinical rehabilitative approaches that focus on strength. The local tissue has probably improved in its characteristics (tendon mechanical properties, muscle strength); however, the drive to the muscle has not been addressed due to the nature of self-paced resistance training; thus, the outcome may still be undesired (perhaps in terms of recurrence). (C) In this example, the focus may be purely on trying to alter the biomechanics or motor control with repetition and feedback about the task (eg, proprioception exercises). This not only has been shown to have poor integration into the sporting environment, it also has not addressed the tissue capacity. Therefore, the local feedback to the central nervous system is likely to maintain the motor control pattern as an ongoing protective or adaptive strategy. (D) The concept of tendon neuroplastic training includes using strength training to address the tendon as load is the only stimulus shown to promote the matrix. Furthermore, strength training improves muscle architecture. In this example, the external pacing of strength training also serves to address cortical muscle control in an attempt to improve the muscle recruitment pattern and therefore, also tendon load.

Figure 2 Individual weekly response to tendon neuroplastic training (isometric protocol). Mean±SEM MEP amplitude (note error bars are too small to be seen; MEP, motor evoked potential).
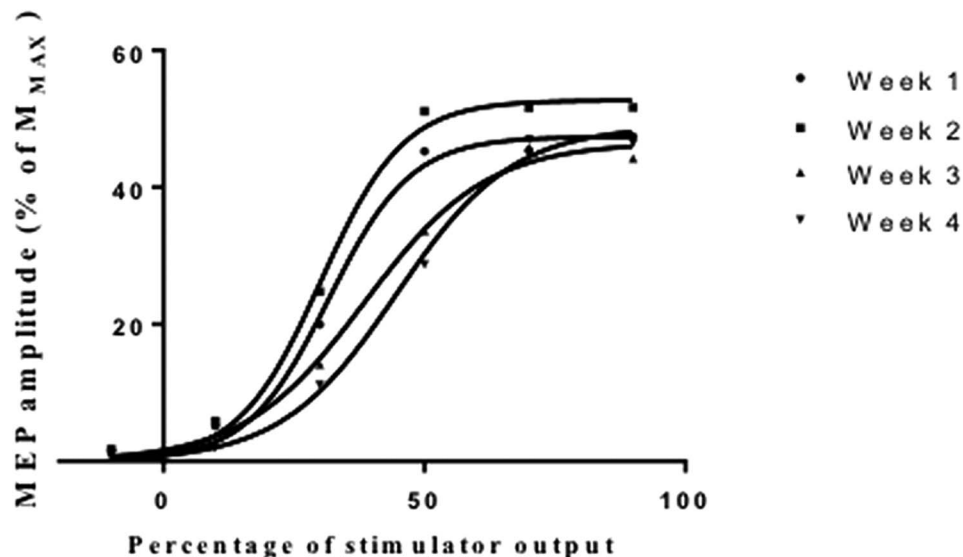
Preliminary data for the individuals and group responses are provided. The values are a percentage representing cortical inhibition of the quadriceps where normative values (for those without PT) are 50–70%.[11] [26] All athletes improved to be within the normal range following the intervention; hence, this represents a physiologically important change. There were differences between the isometric and isotonic group (figure 3); however, clinical implications are limited based on small sample size. Furthermore, a larger study that compared self-paced with externally paced would elucidate if the effects are associated with a reduction in nociception or the use of external pacing or a combination. Data in healthy participants would support the use of external pacing over self-pacing in targeting the M1 and given the nociception-motor interactions,[48] external pacing may augment changes.

CONCLUSION AND CLINICAL IMPLICATIONS

Self-paced strength training targeted to improving muscle architecture describes the parameters of most clinical rehabilitation programmes for tendinopathy. These may not adequately address the differences in excitability and inhibition that has been observed in PT and may be a feature of other tendinopathies. The alterations to corticospinal control of muscle may manifest as a different motor strategy (for protection); however, this could contribute to ongoing morbidity or vulnerability to symptom recurrence. Movement variability appears an important factor in chronicity, yet it is not commonly considered in musculoskeletal pain conditions and may be relevant even if nociceptive input is absent. Aberrant tendon load from altered motor control may be transmitted to tendon causing perpetuation of nociceptive input. However, the altered pattern also
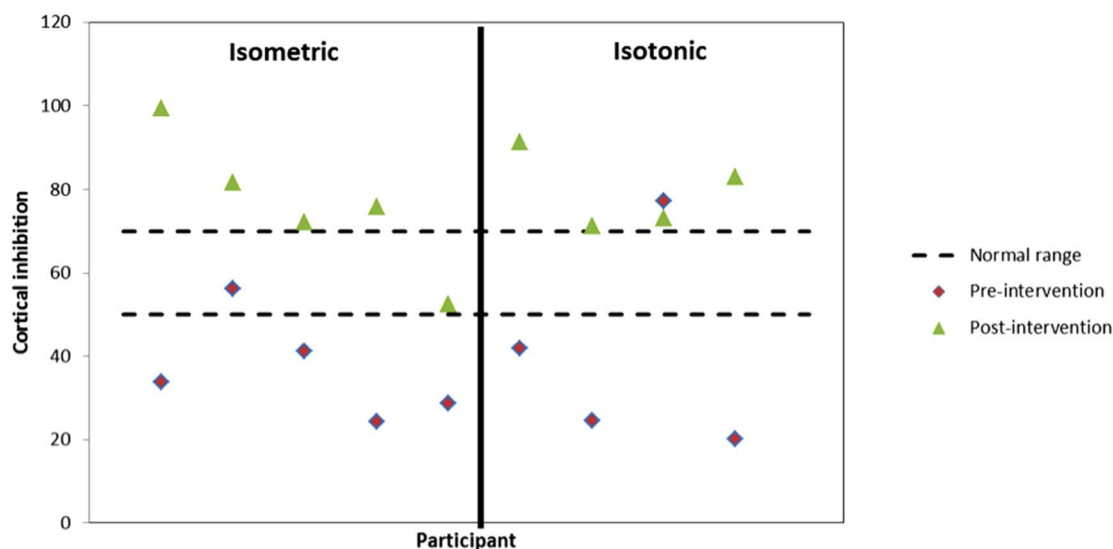

Figure 3 Individual cortical inhibition responses to tendon neuroplastic training by muscle contraction type. Isometric: p=0.06, isotonic: p=0.25, TNT group including both paradigms: p=0.008. Each individual participant's data are provided with diamond denoting preintervention and triangle denoting postintervention for that person.

appears to serve the desire for performance because many studies demonstrate that people with tendinopathy display superior strength or performance. Current rehabilitation for tendinopathy focuses on strength training because it stimulates the physiological adaptation of muscle and tendon. However, strength training that is externally paced has also been shown to be able to modulate tendon pain and corticospinal control of muscle. The concept of TNT incorporates loading that has been shown to be efficacious both in the short and longer term for tendinopathy (4 weeks; Rio *et al*, in submission), in a pain-free protocol which is tolerated by athletes in a competitive environment, as well as those parameters that promote changes to corticospinal muscle control. The current programme may induce change by reducing tendon pain. As clinicians and scientists, it is important that we progress our understanding of the mechanisms behind improvements (or lack thereof) to improve patient outcomes in tendinopathy. This will need to also consider rehabilitation that addresses the unaffected side, which appears to display motor adaptations. How belief systems may impact the prognosis of people with tendinopathy also needs to be explored.

What are the findings?

- ▶ Tendinopathy may be associated with changes in motor control; these changes may be bilateral and persistent despite rehabilitation.
- ▶ Current rehabilitation may not adequately address motor control issues as self-paced strength training (the mainstay of the treatment) does not alter corticospinal drive to the muscle—this may contribute to recalcitrance and recurrence of tendinopathy.
- ▶ Tendon neuroplastic training proposes a concept of strength-based loading that is an important stimulus for tendon and muscle, but with strategies known to optimise neuroplasticity of the motor cortex and drive to the muscle. It needs to be tested in a wide range of anatomical locations as it is unclear whether findings for the patellar tendon are applicable to all tendinopathies.

Ethics approval MUREC.

Provenance and peer review Not commissioned; externally peer reviewed.

Data sharing statement Unpublished data that contribute to the concept provided in this review are available as an online supplementary material. This includes pilot testing as well as further information about the intervention for clinicians and researchers.

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Supplementary file

Method

Preliminary data contained in this supplementary file were collected using the method described below. Participants were recruited from sub-elite and elite basketball and volleyball populations and were aged over 18 years and all playing / training three times per week. If they were not able to participate in games and trainings three times per week for any reason including PT, they were not included because of the potential for activity to modify the primary motor cortex (M1) and motor control as demonstrated in pilot testing.

While habitual activity has been shown to effect the M1, no study was identified that specifically considered the type of activity and the influence on the M1 and motor drive. Thirteen physically active, healthy participants were recruited (Table 1.) All participants completed at least three sessions per week of structured activity and included a mix of elite, sub-elite and recreational athletes. Athletes nominated their dominant leg for testing and the contralateral corticospinal excitability was tested

Table 1 Characteristics of participants in the pilot study that investigated the influence of jumping on corticospinal excitability

Characteristics	Description
N (men)	13 (9)
Age years (median+range)	26 (21-37)

BMI (mean±SD)	23.87±2.60
Weekly activity	Australian football, swimming, touch football, running, martial arts, volleyball and badminton

BMI, body mass index

Following testing, participants were grouped according to activity type (jumping yes/no). Data were coded and all data were analysed blinded to group activity type (Table 2). Stimulus response curves were constructed (normalised to M_{MAX}) and the slope was calculated using GraphPad Prism. Data for M_{MAX}, active motor threshold (AMT) and maximal voluntary isometric contraction (MVIC) are presented as median and range. In order to be conservative, non-parametric analyses (Mann Whitney U) were conducted on all comparisons, as the sample size was small and groups were an uneven number. Physically active people who did not participate in sports that have a jumping requirement exhibited lower corticospinal excitability, evidenced by a decrease in the slope of the stimulus response curve (higher number indicates decrease in slope) (Table 2).

Table 2 Corticospinal responses, peripheral measures and descriptions of each group

Group by activity (jumping yes / no)	Characteristics	M_{MAX}	AMT	MVIC	Slope (AU)
N=8 jumping participants (median+range)	6 men	24.61	42	172.5	5.91
	Australian football	(21.84-27.68)	(31-50)	(152-274)	(4.08-7.90)
	Martial arts				
	Volleyball				
	Badminton				
N=5 non-jumping participants (median+range)	3 men	21.51	35	168	14.04*
	Swimming	(18.7-27.46)	(31-50)	(105-183)	(9.66-17.69)
	Touch football				
	Running				

AMT, active motor threshold; MVIC, Maximum voluntary isometric contraction; AU, arbitrary units * denotes p=0.002

These data suggest that jumping has a profound effect on the CSE and that it is therefore important that any comparisons made between controls, those with other AKP or PT participate in jumping sports. Data were checked for the potential effect of gender and found to be non-significant (p = 0.26). There were no differences between groups for M_{MAX}, AMT or MVIC (p < 0.05).

Based upon these data, the decision was made to recruit both men and women but only include athletes that played / trained at least three times per week in jumping sports in all studies.

Note that the larger randomised clinical trial (RCT) (Rio et al., unpublished data and van Ark et al., unpublished data) included participants aged over 16 years however, only participants aged over 18 years were offered transcranial magnetic stimulation (TMS) testing.

Athletes were asked to complete a VISA-P, a questionnaire about patellar tendon pain and function that is scored between 0 and 100 with 100 being maximal pain free function [1]. Height in centimetres (cm) using a stadiometer and weight in kilograms (kg) without foot ware were recorded and this has been described previously [2].

Clinical diagnosis of patellar tendinopathy

Patellar tendinopathy (PT) in all studies was diagnosed as localised pain at the inferior pole of the patella during jumping and landing as well as during the single leg decline squat (SLDS), a reliable patellar tendon pain provocation test [3]. Grey scale ultrasound (US) was used to confirm the diagnosis by applying the following where at least one criterion had to be satisfied; presence of a hypoechoic area, increased thickness of the anterior/posterior diameter greater than six millimetres (mm) or the presence of vessels. Athletes with bilateral symptoms were asked to nominate their most painful knee on the SLDS using a numerical rating scale (NMR) 0-10 and measures of quadriceps torque were taken from this side only and the contralateral hemisphere was tested with TMS.

Inter-person data

Jumping athletes were recruited and offered bilateral TMS testing. Following testing, they were assessed clinically and using US to determine the presence of tendon pain (NRS pain on SLDS) and tendon pathology (US) for sub-grouping into unilateral or bilateral tendon pain or pathology.

In-season intervention study - Tendon neuroplastic training

Concealed randomisation was achieved by asking the athlete to draw an opaque sealed envelope with no external markings [4]. The envelope contained a number (either one = isometric or two = isotonic) produced by random number generation (Excel 2007©).

Data were collected as part of a RCT with two intervention arms completed over four weeks during a competitive season. The intervention was completed four times per week. There were two active intervention arms, either isometric or isotonic muscle contractions and no sham group. Exercises were completed on a leg extension machine (Figure 1).

Figure 1. An example of a leg extension machine used for the intervention of quadriceps muscle contractions

Both protocols were matched for time under load and rest between sets (set at two minutes to allow muscle recovery) (Table 3) [5]. Repetition maximum (for the isotonic group) and MVIC (for the isometric group) were determined for starting loads. As muscle work during isometric exercise and isotonic exercise cannot be directly measured, protocols were matched for rating of perceived exertion on the basis of pilot studies and to avoid delayed onset muscle soreness as this was an in season study and muscle pain may negatively affect compliance or sporting participation. Furthermore, the protocol were matched for time under tension and based upon data supporting the use of external pacing to modulate corticospinal excitability and inhibition.

Auditory cues have been shown to be beneficial on the induction of neuroplasticity [6-11]. Therefore both groups received an auditory file to play on their smart phone device during their exercise sessions that provided verbal instructions and paced the muscle contractions (Table 3). The aims of this were to try to ensure timing was adhered to, provide auditory stimulation and avoid self-pacing so that the only difference between groups was muscle contraction type.

Table 3. Protocol used in the randomised clinical trial

	Isometric group	Isotonic group
Time under tension	5 x 45 seconds = 225 seconds	4 x 8 3 seconds concentric and 4 seconds eccentric phase = 224 seconds
Starting load	80% MVIC	80%8RM
Progression	2.5% as able	2.5% as able
External pacing and cues	Metronome and verbal instructions	Metronome and verbal instructions
Equipment	Leg extension machine	Leg extension machine
Range	60 degrees	Comfortable range 10 degrees – 100 degrees

Note: the protocol was modified from [2] to prevent delayed onset muscle soreness.

Transcranial magnetic stimulation

Single pulse TMS was used to obtain stimulus response curves and paired pulse TMS technique was used to quantify SICI and these methods have been published elsewhere [2].

Outcome measures and statistical tests

For the inter-person study, outcome measures were active motor threshold, CSE and SICI. For the RCT, outcome measures were short interval cortical inhibition (SICI) and VISA-P. Non-parametric tests were chosen due to small sample size.

Results of the inter-person study

Bilateral data was obtained for 16 athletes (32 hemispheres). Of these, four were control participants recruited to compare SICI against the published physiological normal range for the quadriceps (50-70%) [6, 12] as it was unknown if SICI may be altered in jumping athletes. The median SICI ratio for both sides of control athletes was 56.81 (range 50.86-58.81) and there were no differences between hemispheres in control participants ($p=0.49$). There were no differences between sides in control participants for the slope of the stimulus response curve, left = 7.28, n=4, right = 9.55, n=4, $p=0.83$. This supported data obtained in previous studies of control participants (Rio et al., 2015 accepted) and previously published physiological ranges [12]. Two athletes for whom bilateral data was obtained were excluded (one swimmer and one rock climber). This was because significant differences were found in corticospinal excitability of athletes that regularly jumped and those that did not despite the same number of structured physical activity sessions in a week, in a pilot study of 13 athletes ($p=0.002$). Therefore, fourteen athletes were included in the data provided in the paper, n=4 controls and n=10 with tendinopathy.

The following sub-groups emerged: -

Unilateral tendinopathy (unilateral pain with unilateral pathology) n=3

Bilateral tendinopathy (bilateral pain and pathology) n=2

Unilateral tendinopathy (unilateral pain with bilateral pathology) n=5.

Therefore, the question posed was - what is the effect of unilateral pain on the other side (n=8)?

Results from randomised clinical trial – tendon neuroplastic training

Nine athletes (seven men and two women) with either unilateral (n=5) or bilateral (n=4) PT who were taking no medication were included in the study (Table 2). This was part of a larger trial of 29 people, who were all offered inclusion in the TMS component. Nine athletes completed the study, four in the isotonic group and five in the isometric group.

Table 2. Baseline characteristics and testing

	intervention	LOT sx	height	weight	BMI	KTW L	KTW R	VISA	Leg	SLDS	MVC	AMT	M wave	curve	V50	SICI
												Baseline			
M	isotonic	84	181.5	74	22.464	11	7	69	R	8	202	26	26.519	0.1004	1.701	41.87
M	isometric	24	185	81	23.667	13	8	13	R	7	113	28	18.64	0.2165	1.454	33.82
F	isometric	1	178	65.3	20.61	12	11	65.5	R	5	177	33	15.482	0.2368	1.68	56.3
F	isotonic	24	170.5	100.9	34.709	12	9	46	L	7	220	29	18.381	0.1493	1.475	24.65
M	isometric	36	188	81.1	22.946	12	11	76	R	7	165	36	22.354	0.1283	1.414	41.12
M	isotonic	4	183	79.7	23.799	17	16	65	L	5	263	25	17.474	0.1242	1.389	79.74
M	isometric	36	182.6	84.1	25.223	7	8	63	L	7	152	35	24.29	0.1239	1.452	28.61

M	isotonic	120	194	96.5	25.64	17	17	65	R	9	221	38	22.824	0.1237	1.443	20.17
GROUP		30	182.8	81.05	23.733	12	10	65		7	189.5	31	18.64	0.1283	1.454	41.12

M, male. F, female. LOT sx, length of time of symptoms (months). BMI, body mass index. KTW, knee to wall (cm). SLDS, single leg decline squat. MVC, maximal voluntary isometric contraction. AMT, active motor threshold. Mwave, maximal compound wave. SICI, short interval cortical inhibition

The individual data is provided (Table 3,4) including calculated change scores for the outcome measures – VISA-P, SLDS, SICI. Median and mean are provided, though non-parametric tests were chosen due to small sample size.

Table 3. Individual post intervention data

	VISA	SLDS	MVC	AMT	M wave	curve	V50	SICI
Isotonic	67	3	268	23	25.39207	0.05295	1.791	91.36862
	59	4	228	27	21.98545	0.2336	1.74	71.2662
	84	1	244	25	19.03453	0.1124	1.445	72.98601
	73	3	280	30	24.72848	0.07267	1.532	82.97635
Median	70	3	256	26	23.35697	0.092535	1.636	77.98118
Mean	70.75	2.75	255	26.25	22.78513	0.117905	1.627	79.64929
Isometric	41	4	165	26	20.78287	0.2308	3.483	99.44911

97.5	2	188	33	16.67	0.335	1.934	81.55782
84	4	229	33	19.98445	0.1536	1.407	72.11755
72	2	264	35	21.254	0.245	1.478	75.788
78	3	210	33	20.42	0.247	1.71	52.44907
Median 78	3	208.5	33	20.38366	0.2379	1.706	75.788
Mean 73.625	3	211.5	31.75	19.67283	0.2411	2.0755	76.27231

MVC, maximal voluntary isometric contraction. AMT, active motor threshold. Mwave, maximal compound wave. SICI, short interval cortical

inhibition

Table 4. Change scores pre and post intervention

	VISA	SLDS	MVC	% MVC change	AMT	M wave	curve	V50	SICI
Isotonic	-2	5	66	32.67327	-3	-1.12718	-0.04745	0.09	49.49833
	13	3	8	3.636364	-2	3.604896	0.0843	0.265	46.61606
	19	4	67.82	25.78707	0	1.56073	-0.0118	0.056	-4.32399
	8	6	59	26.69683	-8	1.904929	-0.05103	0.089	62.81073
Median	10.5	4.5	62.5	26.24195	-2.5	1.732829	-0.02963	0.0895	46.61606

Isometric	28	3	52	46.0177	-2	2.142729	0.0143	2.029	65.6265
	32	3	11	6.214689	0	1.18803	0.0982	0.254	25.25372
	8	3	64	38.78788	-3	-2.36908	0.0253	-0.007	30.9979
	9	5	28	13.7931	-2.5	1.665379	0.0198	1.1415	56.12128
	15	4	30	16.66667	0	-0.16	0.074	0.245	23.84107
Median	18.5	3	40	26.29049	-2.25	1.426704	0.02255	0.69775	43.55959

The individual SICI data following the RCT is provided (Table AA5).

Table AA5. Individual pre and post cortical inhibition

	Pre (%)	Post (%)	Change (%)
Isometric	33.82	99.45	65.63

1

2	56.30	81.56	25.25
3	41.12	72.12	31.00
4	24.26	75.79	56.12
5	28.61	52.45	23.84
Group median	33.82	75.79	43.56^
Isotonic	41.87	91.36862	49.49833
1	24.65	71.2662	46.61606
2	77.31	72.98601	-4.32399
3	20.17	82.97635	62.81073
4			
Group median	33.26	77.98	46.62#

^ p=0.06, # p=0.25

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